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Intermediate to long-term results of periacetabular osteotomy in patients younger and older than forty years of age

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INTERMEDIATE TO LONG-TERM RESULTS AFTER HYBRID TOTAL HIP ARTHROPLASTY FOR PATIENTS WITH RHEUMATOID ARTHRITIS

4 Abstract

5	There have been few reports describing intermediate to long-term results after hybrid total hip
6	arthroplasty in patients with rheumatoid arthritis. We followed 52 hips in 44 patients, 5 men
7	and 39 women, for a mean of 11.5 years (range, 5–23.5 years). Revisions had been
8	performed in 6 hips in 6 patients: 1 both acetabular and femoral components for infection, 1
9	acetabular component for aseptic loosening, 3 acetabular components for recurrent dislocation,
10	and 1 acetabular component for dislodgement of the polyethylene liner from the metal shell.
11	None of other acetabular or femoral components were revised or found to be loose at the final
12	follow-up. Although postoperative dislocation remains a concern, hybrid total hip
13	arthroplasty had an acceptable result in patients with rheumatoid arthritis.
14	Key words: hybrid total hip arthroplasty, rheumatoid arthritis, cementless acetabular
15	component, cemented femoral component, clinical results

16 Introduction

17	Rheumatoid arthritis (RA) is a systemic disease characterized by multiple joint involvement.
18	Total hip arthroplasty (THA) has been one of the successful options for patients with RA in
19	terms of pain relief and functional improvement with patient satisfaction. Good results have
20	been reported with use of cemented and uncemented THAs [1-4], however, there have been
21	few reports describing intermediate to long-term results after hybrid THA [5, 6].
22	The hybrid THA combines insertion of an acetabular component without cement
23	and a femoral component with cement. We now assess retrospectively whether a hybrid
24	THA is a viable option for the treatment of patients with RA. We reviewed the intermediate
25	to long-term clinical and radiological results of hybrid THA for non-selected, consecutive
26	patients with RA.

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28 **Patients and methods**

29 Between December 1987 and October 2006, 73 hybrid THAs were performed in 61 patients with either juvenile or adult-onset RA. Nine patients (11 hips) died before a minimum 30 31 5-year follow-up. We were unable to trace 8 patients (10 hips) as a result of refusal to 32 participate, deterioration of health precluding return for assessment, or loss to follow-up. At 33 last follow-up all 21 THAs were radiographically well-fixed at an average of 27 months 34 (range, 6–54 months) postoperatively. We were able to follow-up 44 patients (52 hips, 71%, 36 unilateral, 8 bilateral) for more than 5 years. The average duration of follow-up was 11.5 35 36 years (range, 5–23.5 years). The average age at the time of the index operation was 52.2

37	years (range, 17–74 years). The average weight was 48 kg (range, 35–65 kg) and the
38	average height was 148 cm (range, 130–180 cm). Five patients were men and 39 were
39	women. There were 25 right hips and 27 left hips. According to the functional
40	classification of the American Rheumatism Association, 19 patients had class-II, 23 patients
41	had class-III, and 2 patients had class-IV capacity [7].
42	All of the procedures were performed through the posterolateral approach without
43	trochanteric osteotomy. One of 2 different hybrid THA systems was used. A Harris
44	Precoat, Precoat Plus, or CDH Precoat stem with a titanium hemispherical Harris-Galante
45	porous-coated 1 or 2 acetabular component (Zimmer, Warsaw, Ind) was used in 40 hips, and a
46	4-U Hip System (Nakashima Medical, Japan) was used in 12 hips. The acetabular
47	component was inserted with a line to line fit. An average of 3.4 screws (range, 2–5 screws)
48	was used for fixation. The diameter of the prosthetic femoral head was 22 mm in 40 hips
49	and 26 mm in 12 hips. Standard polyethylene liner was used in 41 and elevated liner was
50	used in 11. The average surface roughness was 2.0 μ m in the Harris Precoat stem, 2.2 μ m in
51	the Harris Precoat Plus or CDH Precoat stem, and 2.0 μm in the proximal half and 1.0 μm in
52	the distal half in the 4-U stem. The surface of the 4-U stem is equivalent to the matte finish.
53	We asked the manufacturers to provide femoral rasps for each final component, which
54	over-rasped by 0.5 mm. All final femoral rasps used in this study for canal preparation
55	over-rasped by 0.5 mm. A so-called second-generation cementing technique was used with
56	Simplex cement (Stryker-Howmedica-Osteonics, Mahwah, NJ) and a cement gun for the
57	retrograde introduction of cement. A methylmethacrylate plug was used in all hips. We did

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not use vacuum-mixing, centrifugation, proximal cement pressurizers, or stem centralizers.

59 We did not repair of the external rotators and the posterior aspect of the capsule.

- 60 Clinical evaluations were made using hip scoring system [8]. Hips with the score of 90 to 100 points were defined as showing excellent results, 80 to 89 points as good results, 61 62 70 to 79 points as fair results and less than 70 points as poor results. An anteroposterior 63 radiograph and a true lateral radiograph were made preoperatively and at each follow-up 64 examination. Anteversion of the acetabular component was measured [9]. The acetabular 65 interface on the anteroposterior radiograph was divided into three zones [10]. The 66 acetabular component was classified as migrated if there was a change of at least 4 mm in the 67 horizontal or vertical position of the center of the component [11]. Linear head penetration into the polyethylene liner was measured [12]. Anteversion of the femoral component was 68 69 calculated by the anteversion angle measured on true lateral radiographs and the neck-shaft 70 angle of each femoral component [13]. 71 Cementing of the femoral stem was classified as Grade A, B, C-1, C-2, and D [14]. 72 The dimensions and location of radiolucent lines at the bone-cement interface of the femoral 73 component and osteolytic lesions were recorded [15]. The canal filling ratio of the femoral 74 component was defined as the percentage of component width to intramedullary width at the
- surgery [16]. Loosening of the femoral component was defined using the criteria described

midpoint of the component on an anteroposterior radiograph taken within one month after

77 by Harris et al. [17].

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The study design was approved by the Ethics Committee of Asahikawa Medical

79 University.

80	Statistical analyses were performed using SPSS software (SPSS Inc., Chicago, Ill).
81	Clinical, radiographic, and surgical factors were evaluated with use of chi-square tests or
82	Mann-Whitney U test where appropriate. Preoperative and postoperative Harris hip scores
83	were compared with use of the Wilcoxon signed-rank test. Probability values less than 0.05
84	were considered significant. Kaplan-Meier survival curves with end points defined as
85	revision for any reason and aseptic loosening of the acetabular and femoral component were
86	calculated. All survivorship data were reported with 95% confidence interval.
87	
88	Results
89	At the time of the most recent follow-up, revisions had been performed in 6 hips in 6 patients.
90	Both acetabular and femoral components of 1 hip with postoperative infection were
91	simultaneously removed 3 months after index surgery. One acetabular component was
92	revised for aseptic loosening 4 years postoperatively. Three acetabular components were
93	revised for recurrent dislocation 2 months, 7 months and 3 years postoperatively, respectively.
94	One acetabular component was revised for dislodgement of the polyethylene liner from the
95	metal shell 9 years postoperatively. None of other acetabular or femoral components were
96	revised or found to be definitely loose at the final follow-up (Fig. 1). Kaplan-Meier analysis
97	revealed that a 10-year survival rate was 98.1% (95% confidence interval: 96.2%-100%) with
98	revision for aseptic loosening of the acetabular or femoral component as the end point and
99	89.5% (95% confidence interval: 85.0%–94.0%) with revision for any reason as the end point,

100	and a 20-year survival rate was 98.1% (95% confidence interval: 96.2%-100%) with revision
101	for aseptic loosening of the acetabular or femoral component as the end point and 85.4%
102	(95% confidence interval: 79.5%–91.3%) with revision for any reason as the end point.
103	The Harris hip score increased from a preoperative average of 37 points (range,
104	22-62 points), to 75 points (range, 46-96 points) at the most recent follow-up for patients
105	who did not have a subsequent revision ($p < 0.001$). The result was excellent in 5 (10%)
106	hips, good in 11 (21%) hips, fair in 23 (44%) hips, and poor in 13 (25%) hips.
107	The average angle of abduction of acetabular components at the latest follow-up
108	was 43.8° (range, 38–60°). The average anteversion of the acetabular components was 13.2°
109	(range, 2–30°) and the average combined anteversion of the acetabular and femoral
110	components was 48.2° (range, 22–80°). None of the acetabular components showed
111	radiographic migration, rotation, or a continuous radiolucent line other than one component
112	which underwent subsequent revision for aseptic loosening. Radiolucent lines were
113	observed around 7 (14%) acetabular components. These lines were all 1 mm wide or less
114	and no sockets showed a continuous radiolucent line. Small pelvic osteolytic lesions were
115	observed adjacent to the acetabular component in 12 (23%) hips. The average rate of head
116	penetration into the polyethylene liner was 0.08 mm (range, 0.01–0.38 mm) per year.
117	None of the femoral components showed definite or probable loosening at the most
118	recent follow-up. The position of inserted femoral components was neutral in 45, varus in 4
119	and valgus in 3. The cementing of the femoral component was grade A in 16, grade B in 24,
120	grade C-1 in 8, and grade C-2 in 4. Grade C-1 was given mainly due to the presence of

121	small voids and grade C-2 due to the presence of a thin mantle of cement. Radiolucent lines
122	were observed around 4 (8%) femoral components. All radiolucent lines were seen at the
123	bone-cement interface located in the zone 1. No radiolucent line was observed at the
124	implant-cement interface. No hips showed femoral osteolysis other than 1 hip with
125	postoperative infection. The average canal filling ratio was 77% (range, 61%–92%).
126	Eight hips (15%) dislocated posteriorly. Three hips had undergone revision of the
127	acetabular component for recurrent dislocation as described. The remaining dislocations
128	were successfully treated without reoperation. The average anteversion angle of the
129	acetabular component in 8 hips with dislocation and 44 hips without dislocation was 11.6°
130	(range, $2-24^{\circ}$) and 13.4° (range, $2-30^{\circ}$), the average anteversion angle of the femoral
131	component was 25.6° (range, 15–35°) and 36.7° (range, 20–65°), and the average combined
132	anteversion angle of the acetabular and femoral components was 37.2° (range, 22-50°) and
133	50.2° (range, 22–80°), respectively. There was a significant relationship between dislocation
134	and anteversion angle of the femoral component ($p = 0.025$), and combined anteversion angle
135	of the acetabular and femoral components ($p = 0.020$). There was no significant relationship
136	between dislocation and patient age ($p = 0.509$), gender ($p = 0.653$), height ($p = 0.257$), body
137	weight (p = 0.775), diameter of the femoral head (p = 0.07), use of elevated liner (p = 0.216),
138	and abduction angle ($p = 0.267$) and anteversion angle ($p = 0.493$) of the acetabular
139	component.

140 There was no intraoperative periprosthetic fracture, nerve palsy, or clinically141 evident pulmonary embolisms.

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143 **Discussion**

144 We previously reported good intermediate-term results of the primary hybrid THA for patients 145 with osteoarthritis secondary to developmental dysplasia [18, 19]. Other authors also 146 reported similar good results of hybrid THAs for patients with developmental dysplasia [20, 147 21]. There have been few reports which described clinical results of hybrid THAs for 148 patients with RA. Lachiewicz and Messick reported average 10-year good clinical results of 149 hybrid THAs, in which operative diagnosis was RA in 15 of 75 hips [5]. Only 1 of 15 cups 150 had radiographic loosening, while all stems had no possible, probable or definite loosening. 151 On the contrary, Bilsel et al reported an average 12-year results of 14 hybrid THAs in patients 152 with juvenile RA, in which 3 of 14 (21%) hips required revision due to cup breakage or 153 aseptic loosening [6]. These results were conflicting, however, a 20-year survival rate of 154 85.4% with revision for any reason as the end point and only 1 acetabular component had 155 aseptic loosening at an average follow-up of 11.5 years in our study, indicating that hybrid 156 THA remains an option for patients with RA.

Whether the results of THAs for patients with RA tend to inferior to those with osteoarthritis (OA) remains controversial. Several studies reported a higher rate of radiologically loose acetabular components in RA with the Charnley prosthesis [22, 23]. Rud-Sørensen et al reported that the overall survival of primary THAs in RA patients is similar to that in OA patients from the Danish Hip Arthroplasty Registry at an average follow-up of 5.9 years [4]. They described that clinical implication of their findings was

163 unclear since the absolute difference in cumulative revision rate estimates between RA and 164 OA patients was small. Furnes et al found no difference in the 10-year survival rate of total 165 implants between RA patients and OA patients [2]. Johnsen et al reported similar results 166 from the Danish Hip Arthroplasty Registry [24]. Our results support these previous studies. 167 Which concept of uncemented, cemented or hybrid THA is better for patients with 168 RA also remains controversial. In several studies, aseptic loosening of cemented cups has 169 been found to be disturbingly high [1, 22, 23, 25-27]. Rud-Sørensen et al did not find such 170 poor results regarding the cemented cups, either due to aseptic loosening or for any cause of 171 revision [4]. Other 2 large registry studies also described good results of the cemented cups 172 [2, 3]. Eskelinen et al reported that there was a trend for better results with the cemented 173 THA concept when all revisions were taken into account, which can be attributed partially to 174 the increased number of liner revisions in the uncemented cup [3]. They found promising 175 results for cemented polyethylene cups, with a 10-year survival of more than 90% and 176 recommended this type of prosthesis as an alternative in younger patients. Furnes et al did 177 not find any significantly worse results of the cemented cups either [2]. These recent good 178 results with cemented cups may have related to several substantial improvements in modern 179 cementing techniques during the past 10-20 years. 180 Eskelinen et al indicated that although uncemented cups do not have any better 181 resistance to aseptic loosening than cemented cups in young patients with RA, press-fit 182 porous-coated uncemented cups were the only concept to show a positive cohort effect, the

183 survival rate for cups implanted during 1992–2003 being higher than that for cups implanted

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184 in 1980–1991 [3]. Highly cross-linked polyethylene and optional surface bearings such as 185 ceramic and metal-on-metal articulations may reduce wear and improve the results for 186 uncemented cups. Long-term results will be required, however, to conclude whether or not 187 they provide a solution for patients with RA. 188 Several authors have reported good results concerning the survival of stems in RA 189 patients [2-4, 28-30]. Modern, second-generation uncemented stems with proximal 190 circumferential porous coating have been reported to be a good choice for young patients with 191 RA [3]. Rud-Sørensen et al reported that the good survival of cemented and uncemented 192 stems in RA patients, supposing that it might be due to a lower level of physical activity in 193 RA patients [4]. On the contrary, although the results of cemented stem fixation with a 194 modern, third-generation cementing technique have been reported markedly better than those 195 with first-generation techniques [31, 32], Eskelinen et al reported that the results of cemented 196 stems did not improve significantly from the 1980s to the 1990s in young patients with RA [3]. 197 The reason for this somewhat conflicting finding remains unclear. There was no aseptic 198 loosening of the cemented stems in our study. Our consistent surgical techniques including 199 "tight-fit technique", in which all final femoral rasps used for canal preparation over-rasped 200 only by 0.5 mm, seem to have contributed to the good clinical results [18, 19]. 201 Several studies have reported increased rates of dislocations in patients with RA. 202 Hedlundh et al described an increased risk ratio of 1.8 for patients with RA compared to those 203 with osteoarthrosis in more than 3000 Charnley hip arthroplasties [33]. Creighton et al 204 reported an 11% dislocation rate in 103 cemented THAs in patients with RA, in which all

205 operations were performed by 1 surgeon through an anterior approach [26]. They used 2 206 types of prosthesis: either a Charnley stem with a 22.25-mm diameter head or an Iowa stem 207 with a 28-mm diameter head. Berry et al performed a retrospective study on more than 6000 208 Charnley THAs operated in the Mayo clinic between 1969 and 1984 [34]. They reported 209 long-term risk of dislocation after THA, in which the 445 patients (622 hips) with 210 inflammatory arthritis had a mildly elevated risk of dislocation compared with the 3498 211 patients (4279 hips) with OA using multivariate analysis. Zwartelé et al carried out a 212 prospective study assessing the incidence of dislocation within 2 years after surgery for patients with inflammatory arthritis and OA [35]. They reported that a dislocation rate in 213 214 patients with inflammatory arthritis was significantly higher than that in patients with OA: 215 10% (7 of 70 hips) in the inflammatory arthritis group and 3% (10 of 340 hips) in the OA 216 group, and emphasized that inflammatory arthritis must be considered to be an independent 217 risk factor for dislocation after primary THA. Our results support these previous studies. 218 The 15% dislocation rate for RA patients found in our study is unacceptably high. Zwartelé 219 et al discussed that the inferior quality of the soft tissues due to RA probably leads to 220 inadequate soft tissue tension, and that the concomitant impairments in RA patients including 221 the upper extremity, ipsilateral knee and ankle or contralateral hip can lead to hyperflexion of 222 the operated hip while rising from a chair, or during other activities of daily living [35]. To 223 reduce the risk of dislocation in patients with RA, they suggested careful intraoperative soft 224 tissue handling to preserve the stabilizing structures, consideration to use an acetabular 225 component with an elevated rim, special attention during the postoperative rehabilitation

226	program to prevent hyperflexion of the operated hip. Our high dislocation rate seems to be
227	related to the use of femoral heads with a relatively small diameter of 22 mm in 40 hips and
228	26 mm in 12 hips. Although the use of elevated liner did not reduce dislocation rate in this
229	study, it might be associated with our small cohort of patients. Our use of the posterior
230	approach without repair of the external rotators and the posterior aspect of the capsule also
231	might have been a factor leading to the high dislocation rate. We agree with the measures
232	proposed by Zwartelé et al to reduce the risk of dislocation in patients with RA.
233	Dislodgement of the polyethylene liner from the metal shell has been reported as a
234	complication of the HGP-I or II component [36, 37]. The locking mechanism for the
235	modular polyethylene liner was greatly improved in the same titanium fiber-coated Trilogy
236	component, which has been commercially available in Japan since 1995.
237	Several clinical studies have shown a high failure rate of the precoated femoral
238	component [38-40]. Ong et al [39] reported that the failure rate of roughened, precoated,
239	cemented femoral components was considerably higher and occurred earlier than that of
240	femoral components that were neither textured nor precoated with methylmethacrylate.
241	These studies suggested that an enhanced cement-prosthesis bond may be deleterious rather
242	than helpful because rougher surfaces generated more cement debris than smooth surfaces
243	when loosening occurred. Use of a precoated or so-called matt finish femoral component in
244	hybrid THAs was not detrimental in intermediate-term results of hybrid THAs in this study
245	with an average follow-up of 11.5 years, however, careful observation over a longer-term
246	follow-up period is indispensable for these components.

247	We conclude that hybrid THAs provides acceptable intermittent to long-term results
248	for patients with RA. Postoperative dislocation remains a concern. Although we do not
249	have any data to reduce the dislocation rate, it might be possible that the use of a larger
250	diameter of the femoral head, acetabular component with an elevated rim, and careful
251	intraoperative soft tissue handling could reduce dislocations. We believe that use of a tight
252	fit technique is important to achieve good clinical results for the cemented femoral component.
253	On the basis of our results, we continue to use the hybrid THA for patients with RA.

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